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(71) Applicant: CHILDREN'S HOSPITAL MEDICAL CENTER  
Elland and Bethesda Avenues  
Cincinnati Ohio 45229(US)

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(72) Inventor: Clark, Leland C., Jr.  
218 Greendale Avenue  
Cincinnati Ohio 45220(US)

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(74) Representative: Allen, Oliver John Richard et al,  
Lloyd Wise, Tregeare & Co. Norman House 105-109  
Strand  
London, WC2R 0AE(GB)

(54) Method of measuring lactic acid in a liquid.

(57) A method of measuring lactic acid or lactate and derivatives thereof in liquids which is extremely versatile and is suitable for use in a number of areas such as the rapid measurement of lactic acid in whole blood, the ratio of lactic acid to pyruvic acid in whole blood, measurement of lactic acid and the study of living lactic acid-producing cells. The acid or lactate is measured by reacting the lactic acid with lactic oxidase to produce pyruvate and H<sub>2</sub>O<sub>2</sub>. The H<sub>2</sub>O<sub>2</sub> is then measured polarographically. The current produced is directly proportional to the lactate level. Preferably, the lactic oxidase is trapped between two semi-permeable membranes. One membrane is placed in contact with an electrolyte at the tip of an electrode and the second membrane contacts the liquid being tested.

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The invention relates to the rapid measurement of lactic acid or lactate in a liquid, and in particular in whole mammalian blood.

Medical science is now realizing the importance of rapidly measuring lactic acid levels in blood, skeletal muscles and the heart. Lactic acid levels in blood appears to be an indication of certain critical features in mammals. A high blood lactic acid level frequently is an indication that a mammal is about to go into shock. For accident victims, it could be extremely critical to rapidly determine the lactic acid level.

Such a determination should be rapid and use minute quantities of blood in order to permit repeated measurements of lactic acid level. In infants, lactic acid levels are important indicators of defects in metabolism of carbohydrates. With infants, sample size is extremely critical since the amount of blood in the infant is substantially less than that of an adult.

Some authorities theorize that the ratio of lactic acid to pyruvic acid in blood is important. Accordingly, any method of measuring lactic acid should preferably also enable one to measure pyruvic acid in order to determine this ratio.

Currently, there are various methods to measure lactic acid. When the lactic acid is measured in whole blood, the plasma generally must be separated from the blood to eliminate undesirable substances 5 which could cause side reactions. For example, the lactic acid has been measured indirectly by reduction using a lactic dehydrogenase which consumes oxygen and the oxygen decrease is thereby measured to indicate lactic acid levels. This is an indirect measurement 10 of lactic acid and tends to be extremely expensive and time consuming. In these reactions, the blood is separated from the lactic dehydrogenase by using a semi-permeable membrane. Other methods include colorimetric methods in which the blood plasma is 15 separated from the whole blood cells using filtration or centrifugation to separate the whole blood cells from the plasma. The plasma can then be reacted with lactic oxidase to produce hydrogen peroxide which can be colorimetrically measured. These methods are time 20 consuming and expensive and fail to provide a means to rapidly detect lactic acid directly.

Furthermore, these methods fail to provide a means to measure the ratio of lactic acid to pyruvic acid and further fail in that they do not provide a 25 means to measure in situ lactic acid levels. This would be particularly important in measuring lactic acid levels in the heart.

About 15 years ago, enzyme-coupled electrodes were reported for the polarographic analysis of the 30 substances. For example, U.S. Patent No. 3,539,455

discloses a membrane polarographic electrode system method for the rapid and accurate quantitative analysis of substances which theretofore posed difficulties in analysing directly by polarographic 5 methods. According to the description in our mentioned patent, small molecular substances, such as glucose, were measured with a membrane polarographic electrode system. By use of cellulose or another membrane which is permeable to small molecules such as glucose, but 10 impermeable to proteins, the membrane keeps glucose oxidase enzyme on the side of the membrane with the anode for reaction with glucose. Therefore, for example, when a sample of blood were placed on the membrane side opposite the electrode with an aqueous 15 solution of enzyme and oxygen on the electrode side of the membrane, low molecular weight molecules such as glucose pass from the blood samples through the membrane for enzymatic reaction adjacent the electrode. After a certain period of time, a steady 20 state is reached when the hydrogen peroxide concentration is directly proportional to the glucose concentration and the cell produces a current flow as a function of the amount of hydrogen peroxide being formed which serves as an indication of the amount of 25 glucose present.

Lactic oxidase for some time has been puzzling the scientific world. For some time, it was a matter of dispute whether lactic oxidase, in fact, could produce hydrogen peroxide from lactic acid. One 30 possible reason for this dispute is frequently

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the enzyme had associated therewith a substantial amount of a catalase which would quickly consume hydrogen peroxide. A second source of this dispute was the improper characterisation of lactic oxidase.

- 5 Certain enzymes, which were actually lactic oxoreductases, were characterised as lactic oxidases. These lactic oxoreductases, instead of producing hydrogen peroxide and pyruvate from lactic acid, produced acetic acid, carbon dioxide and water.
- 10 However, it has been recently appreciated in the literature that there are true lactic oxidases and which are substantially catalase free and suitable for the reaction to produce hydrogen peroxide from lactic acid or lactate. Such an enzyme is disclosed in U.S.

Patent 4,166,763, assigned to Eastman Kodak Company.

This patent discloses an enzyme for use in analysis of lactic acid whereby the lactic acid is oxidized to produce pyruvate and hydrogen peroxide. The hydrogen 5 peroxide is measured colorimetrically.

In European Patent Application No. 0024155 there is disclosed an apparatus for use in a method for cutaneously measuring substances in the body of a mammal comprising an enzyme implant and analysing means for use on the 10 mammal body.

It is an object of this invention to mitigate or overcome one or more of these above problems.

In accordance with one aspect of the invention a method of measuring lactic acid or derivatives thereof 15 in a liquid comprising reacting the lactic acid or derivative with lactic oxidase to produce pyruvate and hydrogen peroxide and measuring the hydrogen peroxide polarographically.

In accordance with another aspect of the invention 20 a method of analyzing the lactic acid production of cells comprising trapping lactic oxidase between an inner and an outer membrane layer wherein the inner membrane separates the lactic oxidase from an electrolyte solution of a polarographic cell and immobilizing the 25 cells on the outer membrane layer wherein the outer membrane layer permits lactic acid to pass through into the lactic oxidase and the inner membrane permits  $H_2O_2$  to pass through into the electrolyte and polarographically measuring the  $H_2O_2$  which passes through the inner membrane.

The present invention is based upon the realization that lactic oxidase can be used to oxidize lactate or lactic acid to produce pyruvate and hydrogen peroxide and that the hydrogen peroxide can thereby be measured polarographically. Particularly, it has been found that lactic acid can migrate through a membrane into contact with lactic oxidase where it is converted to hydrogen peroxide. The produced hydrogen peroxide will then migrate through a second membrane to an electrode. The decomposition of the hydrogen peroxide will produce a current flow across the cell which can be determined as a measure of rate of formation of the hydrogen peroxide and is an indication of the amount of lactic acid or lactate present in the material under analysis.

A number of advantages are provided by this invention. Lactic acid can be measured directly even when the lactic acid is contained in whole blood which may contain a great deal of catalase. In this situation, the sample does not have to be prepared prior to analysis to eliminate any unwanted contaminants. Thus, a measurement of lactic acid level can be made in about 40 seconds.

In one of its broader aspects, this invention is directed to a method of quantitative polarographic determination of lactic acid which is converted by at least one enzyme to produce hydrogen peroxide. A polarographic cell is provided, including at least one electrode sensitive to

hydrogen peroxide. A sensing electrode is positioned behind a first membrane which is permeable to hydrogen peroxide. Lactic oxidase and potentially additional enzymes are contained between this first membrane and 5 a second membrane which separates the enzyme from the sample. Lactic acid in the sample migrates through the second membrane to react with the lactic oxidase and produce hydrogen peroxide and pyruvate. The hydrogen peroxide then passes through the first 10 membrane into the electrolyte of the cell. Potential is established across the cell and the produced current is proportional to the amount of hydrogen peroxide produced.

In such a membrane polarographic cell, a 15 quantity of material containing lactic acid to be measured is added for enzymatic reaction on the side of the membrane opposite the electrode and to effect diffusion of at least a portion of the hydrogen peroxide into the membrane and into contact with the 20 electrode. Then the current flowing across the cell is determined as a function of the amount of hydrogen peroxide formed and as an indication of the amount of the lactic acid in the material. The current flow is measured as the rate of formation of hydrogen peroxide 25 by enzymatic reaction with the lactic acid. In an embodiment of the present invention, pyruvic oxidase is admixed with the lactic oxidase to react with the formed pyruvic. The pyruvate in the presence of pyruvic oxidase forms acetic acid and hydrogen 30 peroxide. Thus, more hydrogen peroxide is produced from the same amount of lactic acid. This

substantially increases the sensitivity of the detection of lactic acid.

Polarographic cells of this type can be modified to measure the ratio of lactic acid to 5 pyruvic acid. Furthermore, these cells can be added to catheters to measure in-vivo lactic acid levels. These cells can also be modified by immobilisation of 10 various animal, plant or bacterial cells which produce lactic acid onto the outer membrane. This provides a method of observing lactic acid production by these 15 cells. This heretofore unappreciated versatility of such a method of measuring lactic acid is an advantage of the present invention.

The invention will be now described, by way of 15 example, with reference to the accompanying drawings, in which:-

Figure 1 is a diagrammatic illustration of a 20 polarographic instrument and other means employed in the methods of this invention showing the overall arrangement of an electrical circuit, polarographic cell, and the sample chamber;

Figure 2 is an enlarged view of the lower 25 central portion of the polarographic cell of Figure 1 and showing in more detail the laminated membrane of the polarographic cell;

Figure 3 is a plot of current versus time for a whole blood sample, and

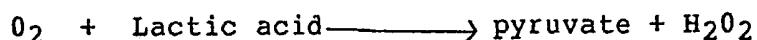
Figure 4 is a typical calibration curve made according to the method of the present invention.

30 Throughout the specification, the term

lactic acid and lactate may be used interchangeably. The present method provides a means to measure lactate, lactic acid as well as lactic acid derivatives which react with lactic oxidase to produce 5 hydrogen peroxide. These derivatives include phenyl lactate and ethyl lactate. The method of the present invention is premised on the following reaction:

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Lactic  
oxidase



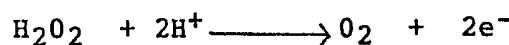
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The hydrogen peroxide is then measured using a membrane polarographic cell of the type shown in Figures 1 and 2 and more particularly, disclosed in our U.S. Patent No. 3,539,455 which is incorporated herein by reference.

20

In the polarographic apparatus of Figure 1, the electrode probe 5 oxidises a constant portion of the hydrogen peroxide at the platinum anode 6 as most probably illustrated by the following reaction:

25



The circuit is completed by silver cathode 7 at which oxygen is reduced to water as most probably illustrated by the following reaction:

5



Relating the above reactions to the principle  
10 of operation in Figure 1 of the drawing, Figure 1 is a  
diagrammatic illustration of an apparatus illustrating  
the polarographic cell 9 with electrode probe 5 and  
sample chamber 8.

In the detailed operation which follows, a  
15 modified Model 23, Yellow Springs Instrument Glucose  
Analyser was employed and is here described as  
follows. The cell is provided with its own potential  
source which in this case is a battery 10 using an  
applied voltage of about 0.7 volts. The positive pole  
20 of the battery is attached to the platinum  
polarographic anode 6 having a face 11 diameter of  
0.5 mm with an adjacent silver chloride coated silver  
wire reference cathode 7 having an active surface area  
of about 0.5 square cm. A full scale output is of the  
25 order magnitude of 100 nanoamperes. A G-2500 varian  
strip chart recorder (not shown) was used to make the  
current measurements. Referring to Figure 1, there is  
shown a cell assembly which includes an electrically

insulating support body 12 of plastic or glass which is preferably cylindrical and which is covered by an electrically insulating cap 14. Positioned within a cylindrical body 12 is an electrically insulating member rod 15 of plastic or glass which supports a platinum electrode, the latter, including an active exposed face 11. The electrode 6 is attached to a battery source 10 by a conductor 18 which passes through rod 15 and through cap 14.

10 The lower end of the support body 12 is provided with an annular ring or retainer 19 and a laminated membrane 20. This laminated membrane is supported over the end of the supporting body nearest the electrode 6 and spaced a capillary distance from the active face 11. The membrane is held in position on the supporting body by an O-ring 21.

15 An annular space is provided between the rod 15 and the supporting body 12 and receives a reference electrode 7 which may be, for example, silver chloride coated silver wire. The space 25 between rod 15 and supporting body 12 is at least partly and preferably completely filled with a liquid mixture of electrolyte which contains both electrodes 7 and 6 and which may be introduced in the chamber through an aperture 31 provided beneath the cap 14. Typical electrolytes include sodium or potassium chloride buffers including carbonate, phosphate, bicarbonate, acetates, or alkali or rare earth metals or other organic buffers for mixtures thereof. The solvent for such electrolyte 30 may be water, glycols, glycerine and mixtures thereof.

In the present invention, an aqueous mixture of  $\text{Na}_2\text{HPo}_4$  and  $\text{Na H}_2\text{PO}_4$  is preferably used.

Figure 2 shows membrane 20 more fully and will be referred to primarily in the description of that membrane. Layer 32 as shown is that adjacent the active surface 11 of anode 6. That layer is essentially homogenous silicone, methyl, methacrylate or cellulose acetate material. Layer 34 is the outer layer which will be in contact with the sample to be analysed. In the preferred embodiment, this is a 0.03 micron pore size perforated polycarbonate film having a thickness of 5 microns, nitrogen flow rate of 25 ml/min/cm<sup>2</sup> at the 10 psi and having six  $\times 10^8$  holes per centimetre square. Such films are available from the Nuclepore Filtration Products of Pleasanton, California. When an approximately 5-7 micron thick support film is used, the overall thickness of the laminated membrane is less than 10 microns as is preferred. Typical thickness would be 5 microns for outer layer 34. One micron for inner layer 32 and one micron for the intermediate enzyme layer 36 for a total of 7 microns thickness. Layer 36 is the enzyme material used to react with the lactic acid and/or pyruvate and acts to bond layers 32 and 34 together.

Laminate membrane 20 is preferably produced by first placing the essentially homogenous layer on a strippable carrier sheet. In the case of cellulose acetate, this is done by depositing the cellulose acetate in a solvent, cyclohexanone, for example, onto water. A film forms which can be picked up by a strippable carrier sheet, such as polyethylene.

A similar process can be used for silicones and other essentially homogenous material, such as methyl methacrylate. As mentioned, the preferred thickness for the essentially homogenous layer is in the range 5 of 0.5 to 1.0 microns.

The lactic oxidase preparation may be simply a mixture of lactic oxidase in water. Of course, other materials, such as a binder or a cross linking agent like gluteraldehyde may be included in the enzyme 10 preparation. Likewise, the portion of lactic oxidase to water in the preparation is not material as long as a flowable paste or solution is formed which may be coated or pressed easily into a thin uniform layer, and sufficient enzyme is incorporated by an adequate 15 reactive amount of measurements. About 17-20 U of enzyme provides sufficient enzyme activity to test 10 to 25  $\mu$ l sample having up to about 200 mg/ml lactic acid. The enzyme solution is further discussed below.

After placing the aqueous enzyme solution or 20 paste onto the essentially homogeneous layer, a self-sustaining support sheet of diffusion barrier material 34, preferably a porous polycarbonate is brought into contact with the enzyme preparation on the cellulose acetate layer to form a laminate. The 25 laminate is then dried by allowing it to sit in air at room temperature for a half hour or more. Additionally, to condition the laminate for transit and storage, it may be baked at 45°C for approximately half an hour. When the carrier sheet is removed, the

laminate membranes are ready for installation onto a polarographic cell.

However, if preferred, the laminating procedure may be followed by gluing onto the support 5 layer 34, a rubbery O-ring 21 of an appropriate size for fitting into the retainer 19 on the polarographic cell 10 (see Figure 1). Laminated membranes 20 ready for use may be punched around the O-rings. Of course, the support layer is stripped off the face of the 10 essentially homogenous layer in this case also.

Most significantly, because the laminated membrane may be less than 10 microns in thickness, less than 30 seconds, and in some cases, as few as 10 seconds is taken for a polarographic analysis. During 15 that short period of time, the lactic acid and oxygen diffuse through the layer 34, react with the lactic oxidase in layer 36. Then the hydrogen peroxide formed diffuses through layer 32 to contact the active face 11 of the anode 6. The current reaches a steady 20 state and the measurement of the amount of hydrogen peroxide is made. This quick measurement time is extremely important in laboratories and hospitals for numerous analysis must be made each day. The membrane structure as described above is more fully described 25 in U.S. Patents Nos. 3,979,274 and 4,073,713 which are both incorporated herein by reference.

Positioned at the side of the sample chamber 8 is a thin oxygen-permeable membrane such as silicon rubber which permits the passage of air or oxygen from 30 a stirring pump into the enzyme electrolyte mixture

contained in the sample chamber 8 and the gas is eliminated through the vent. A syringe for injection of a sample is shown with buffer supply, injection port, septum cord and waste removal, thereby 5 illustrating flow of sample analysis.

Critical for the present invention is the use of a proper lactic oxidase capable of catalising the reaction of lactic acid or lactate to form hydrogen peroxide and pyruvate. The lactic oxidase must be 10 substantially catalase-free. Catalase is an enzyme which quickly binds and destroys hydrogen peroxide. Therefore, if substantial quantities of catalase are present, the hydrogen peroxide is consumed prior to reaching the active face of the electrode. Thus, the 15 electrode will not detect any hydrogen peroxide. Therefore, the enzyme should be catalase-free.

The enzyme furthermore, should be water soluble to enable the passage of aqueous solutions of lactic acid into the enzyme. There are several 20 sources of the lactic oxidase. H. J. Eichel and L.T. Roehm in the Journal of Biochemistry, 237, 940-945 (1962) disclosed a bacterium Tetrahymen pyreformis which produces a lactic oxidase which oxidises lactate to pyruvate and hydrogen peroxide. 25 F. B. Cousins, in the Journal of Biochemistry, 64, 297-307 (1956) reports a lactic oxidase which produces pyruvate and hydrogen peroxide from lactic acid derived from Myco smegmatis bacterium. Finally, U.S. Patent 4,166,763 discloses a lactic oxidase obtained 30 from Streptococcus faecalis (atcc 12755) which

oxidises lactic acid or lactate to form pyruvate and hydrogen peroxide. A commercial source of the enzyme is Fermco Biochemicals Inc., which sells a lactic oxidase which is believed to be made by Pediococcus Sp.

5 This is the preferred enzyme. Its catalytic activity may be increased by the addition of flavin adenine dinucleotide (FAD) which is believed to be a coenzyme. As described above in the discussion of the membrane laminate 20, the selected lactic oxidase is  
10 incorporated in the membrane structure of the polarographic cell.

In operation, the membrane polarographic instrument of Figure 1 is used for the quantitative determination of lactic acid or a lactate derivative  
15 which is convertible by lactic oxidase to produce hydrogen peroxide. Aqueous electrolyte and buffer solution is introduced into the sample chamber 8. The lactic oxidase is included in the membrane laminate  
20. The sample under analysis is introduced into  
20 chamber 8 by means of a syringe through the septum cord. Oxygen is provided by the stirring pump through the permeable silicone rubber membrane into the vented sample chamber. As the lactic acid in the sample comes into contact with the outer membrane layer 34,  
25 lactic acid is allowed to diffuse through the membrane layer into the enzyme layer 36. Catalase which may be contained in certain samples such as human blood is prevented from passage through the membrane layer 34 due to the small pore size of layer 34. The lactic  
30 acid or lactate derivative which passes into the

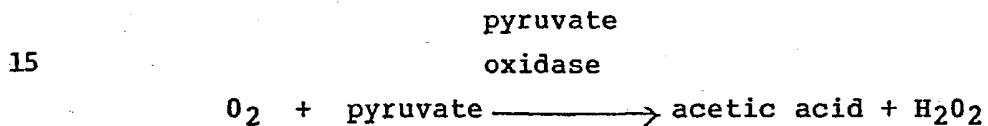
enzyme layer is oxidised to produce hydrogen peroxide which is allowed to migrate through the inner membrane layer 32. This hydrogen peroxide passes across the capillary space 38 between the active face of the 5 anode 11 and the inner membrane layer 32 and causes a current flow. This current flow across the cell is directly proportional to the quantity of hydrogen peroxide diffusing through layers 32. The determination of the current flowing across the cell 10 by the galvanometer 16 is a function of the amount of hydrogen peroxide formed and is an indication of the amount of lactic acid or lactate in the sample. This measurement is a kinetic measurement. Initially, the current is low, but as shown in Figure 3, the current 15 quickly increases and after about 10 to 30 seconds, levels out. At this point, the production of hydrogen peroxide reaches a steady rate which is proportional to the amount of hydrogen peroxide produced. Comparing this current with a calibration curve made 20 using known quantities of lactate as shown in Figure 4, provides the lactic acid level in the sample.

The optimum operating conditions will vary depending on the sample and the source of the enzyme. However, it has been found using the Fermco lactic 25 oxidase that a temperature of about 37°C should be used with a pH of between 6 to 8.

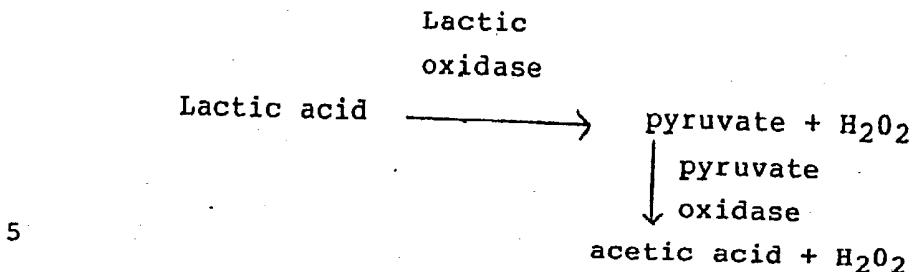
The results shown in both Figure 3 and Figure 4 were obtained using Fermco lactic oxidase without added FAD. The buffer was an aqueous mixture of 30 Na<sub>2</sub>HPO<sub>4</sub> and NaH<sub>2</sub>PO<sub>4</sub> with a pH of 7.28. The

temperature was 37°C. The sample sizes was 25 ul which was injected into a 350 ul cuvet. Using these conditions, linearity is excellent from 0-300 mg/dl if lactate. As stated previously, the life of the enzyme 5 may be increased by adding small amounts of FAD to the buffer.

10 Optionally, pyruvate oxidase can be added to the enzyme layer of the membrane laminate 20 to cause the pyruvate which is produced from the lactic acid to be oxidised to produce hydrogen peroxide and acetic acid. This is demonstrated in the following equation:



Suitable sources of pyruvate oxidase is the enzyme produced by Pediococcus Sp. (EC1 2.3.3.) described in Analytica Chemica Acta 118 (1980) 65-71. Preferably, in this application, equimolar amounts of pyruvate oxidase and lactate oxidase are used in the enzyme layer. The laminate membrane is prepared just as described above with the only exception that the pyruvate oxidase is added. Thus, according to this method, the following reactions take place:



Theoretically, according to this scheme, twice as much hydrogen peroxide is produced from the same amount of

10 lactic acid. This quantitatively increases the amount of hydrogen peroxide produced. Therefore, according to this method, lower amounts of lactic acid or lactate can be detected. It should be noted that this method is not as precise if the sample contains

15 pyruvate.

Medical science has recently considered the importance of the ratio of lactic acid and the pyruvic acid in human blood. This is considered by some to be an important indicator of impending shock. Using the

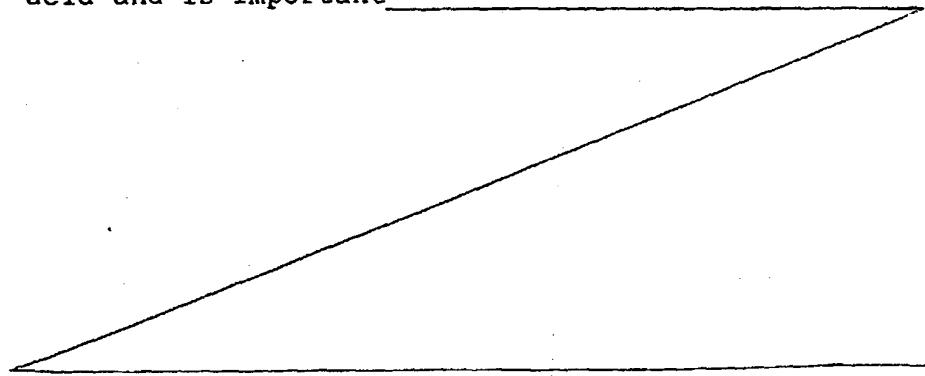
20 previously described method of measuring lactic acid, one can also determine the ratio of lactic acid to pyruvic acid in blood. This modified method is accomplished by using the same previously described method of detecting lactic acid using human whole

25 blood as the sample. After the lactic acid in the human whole blood is measured, lactic dehydrogenase and NADH are injected into the cuvet of the electrode to react with the pyruvic acid in the blood sample. The pyruvic acid reacts with LDH and NADH to produce

30 lactic acid. Accordingly, the lactic acid level will

increase and the current flow will also increase. This increase in current will be caused by the lactic acid derived from pyruvic acid in the blood. Thus, by comparing the initial reading showing lactic acid 5 level in the blood and the second reading showing the increase caused by pyruvic acid in the blood, one can determine the ratio of lactic acid to pyruvic acid. This mechanism of producing lactic acid from pyruvic acid is discussed in Analytica Chemica Acta 118 10 (1980), 65-7. Thus, according to the present method, one cannot only determine the lactic acid in the blood, but the level of pyruvic acid in the blood.

A further use of the method of the present invention is for the observation and study of certain 15 cells which produce lactate. It is known to immobilise a bacteria or other cell in the end of an electrode using glyceraldehyde. The glyceraldehyde and the bacteria are mixed together and physically coated onto the tip of the electrode. Using the method of the 20 present invention, one can place upon the end of the electrode a bacterium such as Lactus Bacillus acidophilus. This bacteria is used to produce lactic acid and is important



## CLAIMS:

1. A method of measuring lactic acid or derivatives thereof in a liquid comprising reacting the lactic acid or derivative with lactic oxidase to produce pyruvate and hydrogen peroxide and measuring the hydrogen peroxide polarographically.
2. A method as claimed in Claim 1 wherein the liquid is whole mammalian blood.
3. A method as claimed in either Claim 1 or 2 wherein the lactic oxidase is trapped between an inner and an outer membrane layer wherein the outer membrane layer separates the liquid from the lactic oxidase and allows lactic acid or derivative to pass therethrough, and the inner membrane separates the lactic oxidase from an electrolyte and allows hydrogen peroxide to pass therethrough and wherein an anode and a cathode are immersed in the electrolyte.
4. A method as claimed in Claim 3 wherein the anode is separated from the inner membrane by a capillary layer of electrolyte.
5. A method as claimed in any preceding claim further comprising contacting the pyruvate with pyruvate oxidase, thereby producing acetic acid and hydrogen peroxide and measuring the produced hydrogen peroxide polarographically.

6. A method of measuring the ratio of lactic acid to pyruvic acid in whole mammalian blood comprising measuring the lactic acid in the blood according to the method claimed in Claim 2, and further comprising

5 adding NADH and lactic dehydrogenase to the blood, thereby converting pyruvic acid in the blood to lactic acid and subsequently measuring the lactic acid in the blood.

7. A method of analyzing the lactic acid production of cells comprising trapping lactic oxidase between an inner and an outer membrane layer wherein the inner membrane separates the lactic oxidase from an electrolyte solution of a polarographic cell and immobilizing the cells on the outer membrane layer

10 wherein the outer membrane layer permits lactic acid to pass through into the lactic oxidase and the inner membrane permits  $H_2O_2$  to pass through into the electrolyte and polarographically measuring the  $H_2O_2$  which passes through the inner membrane.

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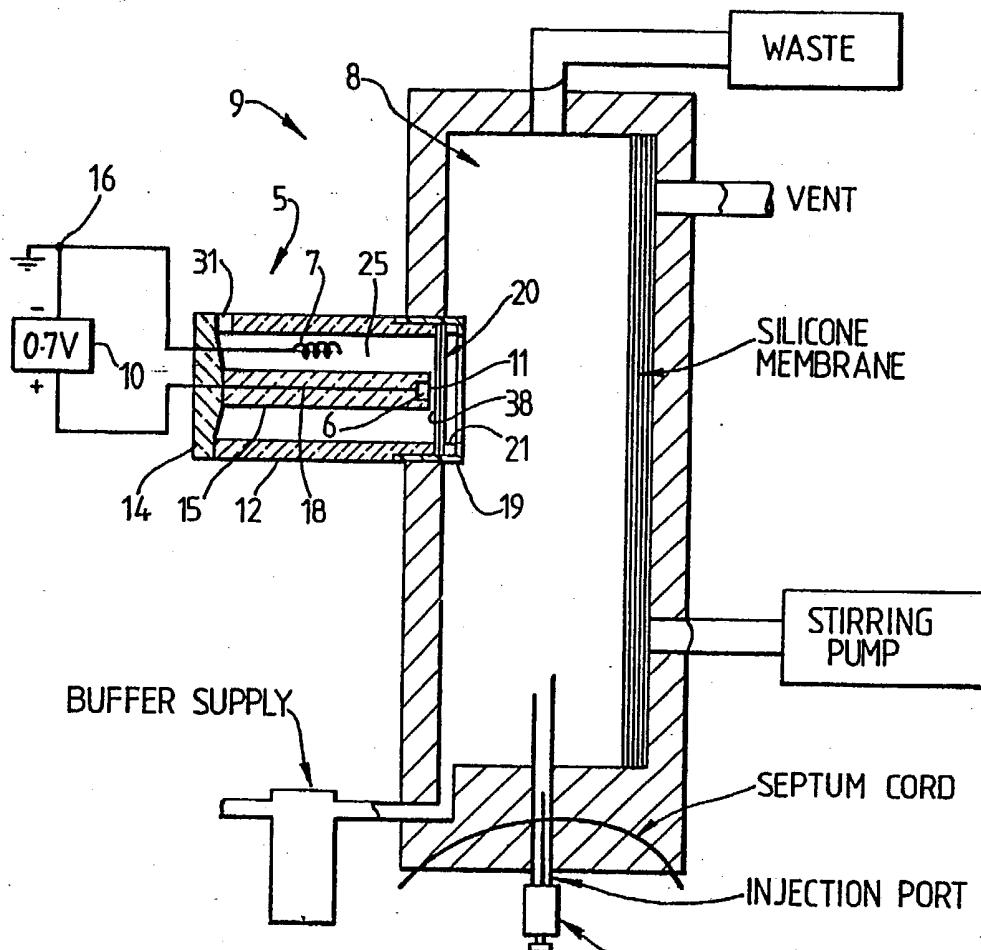


Fig. 1.

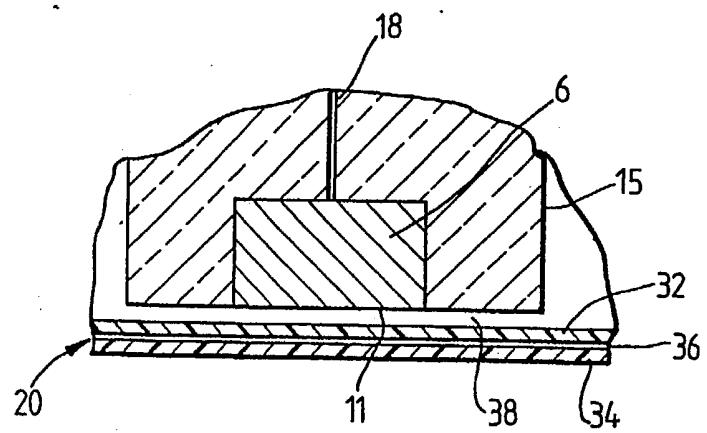


Fig. 2.

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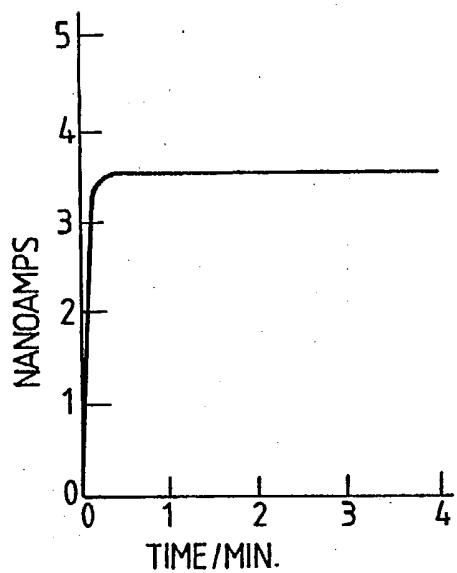


Fig. 3.

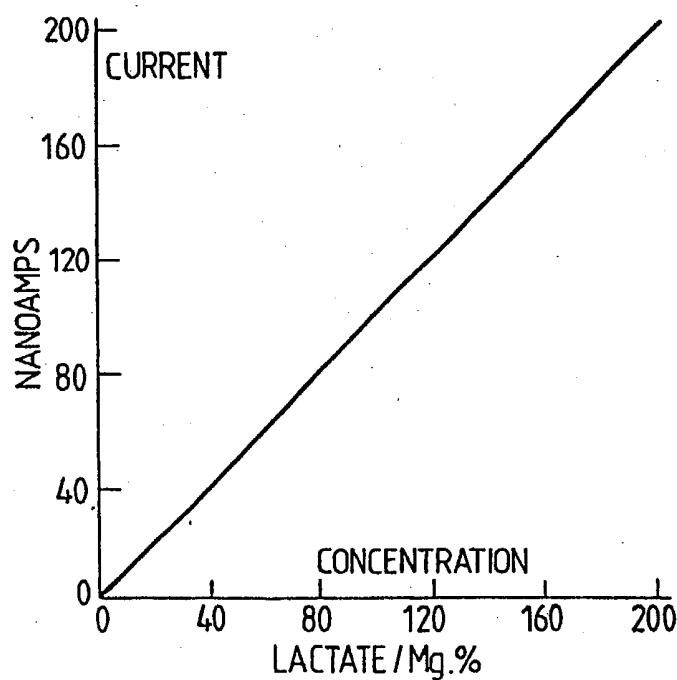


Fig. 4.